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1 **Airborne Aerosol Generation During Endonasal Procedures in the Era of COVID-**
2 **19: Risks and Recommendations**

3
4 **Alan D. Workman MD MTR^{1,2}, Aria Jafari MD^{1,2}, D. Bradley Welling MD PhD^{1,2}, Mark**
5 **A. Varvares MD^{1,2}, Stacey T. Gray MD^{1,2}, Eric H. Holbrook MD^{1,2}, George A.**
6 **Scangas MD^{1,2}, Roy Xiao MD MS^{1,2}, Bob S. Carter MD PhD^{2,3}, William T. Curry**
7 **MD^{2,3}, Benjamin S. Bleier MD FARS FACS^{1,2}**

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9 ¹Department of Otolaryngology, Massachusetts Eye and Ear Infirmary, Boston, MA

10 ²Harvard Medical School, Boston, MA

11 ³Department of Neurosurgery, Massachusetts General Hospital, Boston, MA

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13 Address correspondence to Benjamin S. Bleier MD, Division of Rhinology, Department
14 of Otolaryngology, Massachusetts Eye and Ear Infirmary, 243 Charles St, Boston, MA
15 02215 Benjamin_Bleier@meei.harvard.edu

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17 Conflict of Interest Statement: Dr. Benjamin S. Bleier has consultant relationships with
18 Olympus, Medtronic, Karl Storz, Sinopsys, Baxter, and 3D Matrix and receives royalties
19 from Theime. He holds patents for “Treatment of Sinusitis Through Modulation of Cell
20 Membrane Pumps” (Non-provisional USP assigned to MEEI), “Inhibition of Cystatins for
21 the treatment of Chronic Rhinosinusitis” (Non-provisional USP), and “Methods of delivery
22 pharmaceutical agents” (US 13/561,998). Dr. Bleier is working with industry to develop
23 source control solutions for endoscopic procedures which may include an equity position
24 in the future.

25

26 Key-words: COVID-19, Airborne, Aerosolization, Endoscopy, Nasal Endoscopy, Aerosol
27 Generating Surgery, Aerosol Generating Procedure

28

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30 interpretation of data; ADW and BSB contributed to drafting the work; ADW, AJ, DBW,
31 MAV, STG, EHH, GAS, RX, BSC, WTC, and BSB contributed substantially to conception
32 and design of the work, revision of the draft, and gave final approval for the work.

33

34

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37

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39 **Objective:** In the era of SARS-CoV-2, the risk of infectious airborne aerosol generation
40 during otolaryngologic procedures has been an area of increasing concern. The
41 objective of this investigation was to quantify airborne aerosol production under clinical
42 and surgical conditions and examine efficacy of mask mitigation strategies.

43 **Study Design:** Prospective quantification of airborne aerosol generation during surgical
44 and clinical simulation.

45 **Setting:** Cadaver laboratory and clinical examination room.

46 **Subjects and Methods:** Airborne aerosol quantification with an optical particle sizer
47 was performed in real-time during cadaveric simulated endoscopic surgical conditions,
48 including hand instrumentation, microdebrider use, high-speed drilling, and cautery.
49 Aerosol sampling was additionally performed in simulated clinical and diagnostic
50 settings. All clinical and surgical procedures were evaluated for propensity for significant
51 airborne aerosol generation.

52 **Results:** Hand instrumentation and microdebridement did not produce detectable
53 airborne aerosols in the 1-10 μ m range. Suction drilling at 12,000rpm, high speed drilling
54 (4mm diamond or cutting burs) at 70,000rpm, and transnasal cautery generated
55 significant airborne aerosols ($p<0.001$). In clinical simulations, nasal endoscopy
56 ($p<0.05$), speech($p<0.01$), and sneezing ($p<0.01$) generated 1-10 μ m airborne aerosols.
57 Significant aerosol escape was seen even with utilization of a standard surgical mask
58 ($p<0.05$). Intact and VENT-modified N95 respirator use prevented significant airborne
59 aerosol spread.

60 **Conclusion:** Transnasal drill and cautery use are associated with significant airborne
61 particulate matter production in the 1-10 μ m range under surgical conditions. During
62 simulated clinical activity, airborne aerosol generation was seen during nasal
63 endoscopy, speech, and sneezing. Intact or VENT-modified N95 respirators mitigated
64 airborne aerosol transmission while standard surgical masks did not.

65

66 **Introduction**

67 The COVID-19 pandemic has catalyzed an unparalleled disruption in the provision of
68 health care around the world. Following its detection in December 2019, health policy
69 shifted from an initial strategy of containment to mitigation¹. These efforts have been
70 largely successful at preventing hospital resources from becoming overwhelmed within
71 the United States. However, it has required the delay or cancellation of almost all
72 elective patient visits and procedures. Fortunately, infection and case fatality rates have
73 begun to plateau in even the most severely impacted regions. Clinicians and hospitals
74 now face challenging decisions as to how to safely allow elective patients back into the
75 clinics and operating rooms. This difficulty in planning is further compounded by a
76 persistent lack of personal protective equipment (PPE), effective treatments for COVID-
77 19, COVID-19 testing capacity and turnaround time, and clarity regarding sensitivity and
78 specificity of the currently available tests for COVID-19².

79

80 Rhinologic patients are of unique concern in this reopening phase. Delays in elective
81 care do appear to be associated with worse outcomes³ and higher costs⁴. However,
82 endoscopic procedures have been shown to carry a risk of respiratory droplet formation
83 in both diagnostic and surgical settings⁵. While these risks can be mitigated using low
84 level personal protection equipment, the potential of airborne aerosol generation during
85 endoscopic procedures has not been studied. An evidence-based analysis of this
86 potential is essential as it bears directly on the status of endonasal instrumentation as
87 an Aerosol Generating Procedure (AGP) with its attendant heightened requirements for
88 PPE, air handling, and environmental controls.

89

90 The purpose of this study was to therefore 1) quantify airborne aerosol production
91 following endonasal instrumentation during cadaveric surgical and clinical diagnostic
92 conditions and 2) determine the relative efficacy of source control solutions.

93

94

95 **Methods**

96 *Study Design*

97 The surgical simulation was IRB approved through a formal excess tissue protocol. The
98 clinical simulation was reviewed by the Partner's Human Research Committee director
99 and performed under the Quality Improvement Initiative at Massachusetts Eye and Ear
100 and as such was not required to be formally supervised by the IRB per their policies. All
101 cadaver experiments in this study were performed in a dedicated surgical laboratory
102 using two fresh-frozen cadaver head specimens at room temperature. Both the clinical
103 examination room (111 sq ft) and surgical laboratory (726 sq feet) were equipped with
104 air exchangers operating at a rate of 6 total air changes per hour.

105

106 *Aerosol Sampling*

107 Aerosol sampling was performed using an optical particle sizer (OPS 3330, TSI Inc,
108 Shoreview, MN), which measures particle number, concentration, and size distribution
109 using single particle counting technology up to a size of 10 μ m. Flow rate through the
110 OPS 3330 is a constant 1.0L/min through a 3mm port. Particle size distribution is
111 measured in 16 user-adjustable channels. Total particle counts by size over a period of
112 timed data were collected.

113

114 *Surgical Simulation*

115 The cadaver head was placed in a supine position with the nostril situated 15cm from
116 the optical particle sizer (OPS) intake port (Figure 1A). Five ml of saline was irrigated
117 into the nose using a syringe prior to each surgical condition. For surgical visualization,

118 a high definition endoscopic camera was attached to a 4mm 0° endoscope (Karl Storz,
119 Tuttlingen, Germany). Background samplings were obtained prior to surgical conditions
120 and at least two minutes elapsed between each experiment to allow for verification of
121 return to baseline aerosol concentrations at the intake port. Suction was utilized to
122 evacuate any retained intranasal particulates following all drilling and cautery
123 conditions. Experiments were conducted in 30-second durations with sequential
124 replicates performed for a total duration of 2 to 5 minutes. The surgical conditions
125 included: 1) nasal suctioning using a 10Fr Frazier suction; 2) hand actuated
126 instrumentation using a through cutting forceps of the middle turbinate; 3) powered
127 suction microdebridement (4mm Tricut® blade at 5,000 oscillations/min, Medtronic,
128 Jacksonville, FL) of the posterior nasal septum; 4) powered high-speed drilling of the
129 sphenoid rostrum using a 4mm diamond reverse taper suction drill at 12,000rpm
130 (Medtronic); 5) powered high-speed drilling of the sphenoid rostrum using a Midas Rex
131 Legend Stylus with 4mm diamond bur at 70,000rpm, (Medtronic); 6) powered high-
132 speed drilling of the sphenoid rostrum using a Midas Rex Legend Stylus with 4mm
133 cutting bur at 70,000rpm; and 7) battery-powered endonasal cautery of the inferior
134 turbinate (Acu-Tip, Practicon, Greenville, NC). Each intervention was performed in
135 duplicate on two separate cadaver heads.

136

137 *Clinical Simulation*

138 Subjects were seated upright in a clinical room examination chair with the nare placed
139 15cm from the OPS intake port (Figure 2A). Background samplings were obtained in an
140 empty clinic room, and at least 2 minutes elapsed between experiments to allow for

141 return to baseline aerosol concentrations at the intake port. Each experiment was
142 conducted in 30-second durations with sequential replicates performed for a total
143 duration of 1 minute. The clinical conditions included: 1) simulated heavy mouth
144 breathing (e.g. panting) with breaths every 3 seconds; 2) simulated coughing every 5
145 seconds; 3) speech by reading of the “Rainbow Passage” a standardized vocalization
146 paradigm (Voice and Articulation Drillbook, Harper and Row); 4) simulated sneezing
147 every 10 seconds; 5) simulated nasal endoscopy by the intranasal placement of a
148 2.7mm 0° rigid and 3.5mm flexible endoscope (Karl Storz) for 20 seconds followed by
149 removal; and 6) simulated topical spray of a 1:1 1% lidocaine and oxymetazoline 0.05%
150 solution (MADomizer, Teleflex, Wayne, PA) 15cm away from the OPS intake port every
151 10 seconds. Subjects took a sip of water in between each condition to ensure adequate
152 and consistent hydration. Each intervention was performed in duplicate on two separate
153 subjects.

154

155 Following behavioral simulation, subjects then performed additional simulated sneezing
156 every 10 seconds for 30 second replicates with the opening of their mouth positioned
157 15cm from the OPS intake port, while wearing 1) a Standard Level 1 surgical mask
158 (Halyard Health, Alpharetta, GA), 2) N95 Health Care Particulate Respirator and
159 Surgical Mask (3M 1860, Saint Paul, MN), and 3) modified N95 VENT respirator as
160 previously described⁵ to allow passage of an endoscope through the mask while
161 maintaining a tight seal. An additional trial was performed by doffing of the N95
162 respirator for 30 seconds following sneezing to measure airborne aerosol release
163 following mask removal.

164

165 *Statistical Analysis*

166 Stata version 13 (StataCorp, College Station, TX) software was used for statistical
167 analysis to assess differences between background particle concentration and particles
168 generated during simulated clinical and surgical activities. Non-parametric statistical
169 techniques were utilized due to small sample sizes, with Bonferroni correction for
170 multiple comparisons. Average background particle concentration (separate for clinical
171 encounter and surgical laboratory encounter) was subtracted from each condition prior
172 to data visualization as previously described⁶. Prism Version 8 (GraphPad Software, La
173 Jolla, CA, USA) was used for visualization of data.

174

175

176 **Results**

177 Surgical Simulation

178 *Airborne Aerosol Generation During Cold Instrumentation and Microdebridement*

179 All sampling periods were 30 seconds in duration, and conditions were performed in
180 duplicate with two separate cadaver heads. Sixteen background samples were obtained
181 spaced between experiments and minimal variability in background was observed.

182 Nasal suctioning with a 10Fr Frazier suction for four sampling periods and endoscopic
183 through biting of the middle turbinate (hand actuated) for 10 sampling periods did not
184 produce significant detectable airborne aerosols in the 1-10 μm range (Figure 1B).

185 Application of a microdebrider to the posterior septum with debridement of tissue and
186 declogging external to the nare did not produce 1-10 μm airborne aerosols over 10
187 sampling periods (5 minutes). The cutting edge of the microdebrider was open upon
188 introduction and removal.

189

190 *Airborne Aerosol Generation During High Speed Drilling Conditions*

191 With the cadaver head in surgical position, three separate drilling conditions were
192 performed: (1) a suction drill at 12,000rpm for 10 30-second samples (2) a powered
193 high-speed drill at 70,000rpm with a 4mm diamond bur for 4 30-second samples, and
194 (3) a powered high-speed drill at 70,000rpm with a 4mm cutting bur for 4 30-second
195 samples. The drill was used to remove bone at the sphenoid rostrum. In all three
196 conditions, significant airborne aerosol generation in the 1-10 μm range was observed
197 (Figure 1B; suction drill $p<0.001$, $U=15$, $n=20$; diamond drill $p<0.001$, $U=0$, $n=8$; cutting
198 drill $p<0.001$, $U=1.5$, $n=8$, Mann-Whitney U test). Particle generation was observed to

199 increase throughout the duration of the drilling with increased particle generation during
200 the latter portion of drilling periods. Particle number decreased with increasing particle
201 diameter across the 1-10 μm range (Figure 1C). Finally, an additional experiment was
202 performed demonstrating increased particle generation in the absence of suction using
203 the suction drill at 12,000rpm over the first 120 seconds of drilling (Figure 1D).

204

205 *Airborne Aerosol Generation During Transnasal Cautery*

206 Transnasal cautery of the inferior turbinate demonstrated significant particle generation
207 in the 1-10 μm range over background in 4 30-second samples (Figure 1B, $p<0.001$,
208 $U=0$, $n=8$, Mann-Whitney U test). Particles generated were on average smaller than
209 those observed in the drilling conditions (Figure 1C).

210

211 Clinical Simulation

212 *Airborne Aerosol Generation During Simulated Patient Activities*

213 Subjects were positioned sitting upright with the nose and mouth 15 cm from the
214 aperture of the optical particle sizer air intake valve. All samples were collected over a
215 period of 30 seconds and performed with two different subjects and at least two
216 replicates per subject ($n=4-10$). Panting and coughing generated detectable 1-10 μm
217 aerosols which were not significantly greater than background (Figure 2B). Both nasal
218 endoscopy and speech conditions generated significant airborne aerosols (nasal
219 endoscopy, $p<0.05$, $U=10$, $n=8$; speech, $p<0.01$, $U=6.5$, $n=10$, Mann-Whitney U test).
220 Simulated sneezing generated the most airborne particles per minute by an order of
221 magnitude ($p<0.01$, $U=0$, $n=4$, Mann-Whitney U test). Simulated topical spraying of

222 lidocaine and oxymetazoline generated airborne aerosols comparable to those
223 generated with sneezing (Figure 2C, $p < 0.01$, $U = 0$, $n = 4$, Mann-Whitney U test).

224

225 *Airborne Aerosol Detection During Simulated Sneeze Under Masked Conditions*

226 As simulated sneezing generated the largest number of 1-10 μm airborne aerosols,
227 several sneezing conditions were performed using different source control mask
228 solutions. The surgical mask alone attenuated airborne aerosol generation (Figure 2C),
229 however statistically significant aerosol escape was still detected ($p < 0.05$, $U = 2$, $n = 4$,
230 Mann-Whitney U test). Both an N95 respirator and a modified N95 VENT respirator
231 ameliorated airborne particle generation to background levels. N95 doffing following
232 simulated sneezing over a 30 second period demonstrated an increase in airborne
233 particle generation that did not reach significance above background.

234

235

236 **Discussion**

237 While droplet and contact infectious transmission in SARS-CoV-2 have been largely
238 accepted, the role of airborne transmission remains unclear. This mode is of particular
239 concern in the healthcare setting given the propensity for AGPs to produce particles
240 less than $10\mu\text{m}^7$. The size of the SARS-CoV-2 virus is approximately 60-140nm, based
241 on electron micrographs⁸. Since the advent of COVID-19, the field of Otolaryngology
242 has found itself grappling with potential aerosolization risk of endoscopic procedures
243 despite a distinct lack of quantitative evidence to guide best practices. In an effort to
244 address this unmet need, our team previously reported on a semi-quantitative method
245 to determine the risk of droplet aerosol production during both outpatient diagnostic and
246 surgical endonasal procedures⁵. The purpose of the current study was to extend those
247 findings into the range of airborne aerosols.

248

249 Our surgical simulation conditions were designed to test a variety of endonasal
250 instruments from suction and through cutting forceps through powered devices and
251 thermal cautery. Our findings were generally consistent with our prior study in that use
252 of a surgical drill carried the greatest risk of generating detectable aerosols. The
253 concomitant use of suction appeared to provide some benefit in reducing aerosol
254 concentration however the lower speed of the suction drill is a confounding variable.
255 Similarly, the microdebrider with distal tip suction did not produce detectable aerosols
256 even when requiring removal and active unclogging adjacent to the detector.
257 Conversely, thermal cautery produced significant and particularly fine aerosols which is
258 consistent with the previous literature⁹. These findings serve to provide further evidence

259 that the use of drills and cautery remain the endonasal surgical procedures of greatest
260 risk.

261

262 With regards to the clinical diagnostic conditions, our findings demonstrated that
263 detectable airborne aerosols are generated even during limited periods of speech,
264 panting, cough, and sneeze. However, talking and sneezing were the only behaviors
265 associated with a significant increase over background. Unfortunately, the most
266 common method used to reduce sneezing, namely topical nasal anesthesia and
267 decongestion spray, also produced a significant number of aerosols. While the lack of
268 significance in the other behavioral conditions could be attributed to the short testing
269 duration and use of healthy volunteers, these results are consistent with prior
270 physiologic reports confirming the differential risk of speech and sneeze conditions¹⁰⁻¹³.
271 Of particular importance, unlike our prior droplet data⁵, nasal endoscopy was found to
272 be associated with airborne aerosol production irrespective of whether a rigid or flexible
273 scope was utilized. AGPs are defined by the CDC as “commonly performed medical
274 procedures...that create uncontrolled respiratory secretions.” Insofar as endoscopic
275 examinations 1) require prolonged close proximity to the patient, 2) produce detectable
276 airborne aerosols, and 3) carry a distinct yet unpredictable risk of triggering sneeze
277 events, our findings suggest that nasal endoscopy carries a similar risk profile as
278 currently recognized AGPs⁷¹⁴.

279

280 Our tested mask conditions focused on the ability to mitigate sneeze associated aerosol
281 production as this was clearly the behavior of greatest risk. The existing literature

282 regarding the utility of masks is complex as studies tend to focus on discreet attributes
283 such as filtration efficiency, performance under steady and episodic conditions, or the
284 relationship between mask use and infectious transmission. Epidemiologic and virologic
285 studies have suggested that surgical masks may be equivalent to N95 respirators at
286 protecting healthcare workers from infectious respiratory viruses^{15,16}. Similarly, some
287 virologic reports have shown that surgical masks alone are adequate to prevent
288 coronavirus aerosol spread in both the droplet and airborne ranges during talk and
289 cough conditions¹⁷. Conversely, studies employing episodic stresses such as sneeze
290 have shown that surgical masks are vulnerable to leakage from dynamic changes in
291 pressure and air velocity^{16,18,19}. This is perhaps not surprising as sneezing may produce
292 thousands of airborne droplet nuclei at high speeds^{12,13}. The evident discrepancies
293 between mask efficacy readouts highlights the importance of context dependent testing
294 as a basis for the creation of subspecialty specific safety guidelines. Our results were
295 consistent with previous findings^{16,18,19} in that an intact surgical mask was incapable of
296 controlling the spread of sneeze associated airborne aerosols. This result stands in
297 contrast to our prior findings in which a surgical mask did prevent simulated respiratory
298 droplet contamination⁵. Conversely, the N95 respirator in both the intact and VENT
299 modification conditions appeared to effectively contain aerosol spread. Though not
300 statistically significant, we did observe some contamination after N95 respirator removal
301 suggesting that when used as source control, masks should not be doffed within the
302 clinical space.

303

304 As we apply this data to infection prevention and control recommendations in the
305 outpatient Otolaryngology setting, it is useful to conceptualize the protection needs of
306 the three “Ps”, namely the patient, the provider team (including both administrative and
307 medical staff), and the physical plant (including the clinic/waiting room surfaces and air
308 supply). Comprehensive adherence to “standard precautions” as defined by the CDC¹⁴
309 will tend to simultaneously address each of these groups and should integrate source,
310 engineering, and environmental control strategies. Our results suggest that the proper
311 use of a fit-tested N95 or equivalent VENT respirator is effective at mitigating sneezing,
312 the behavior associated with the highest number of aerosols at the highest velocities.
313 Consequently, these latter barrier strategies may be considered 1) a source control by
314 protecting the provider/physical plant from the patient and 2) an engineering control by
315 protecting the patient from the providers and one another.

316

317 There are several limitations to this study which bear discussion. As the surgical
318 simulation was performed in a cadaver head, it is possible that the lack of pulsatile
319 blood supply at body temperature and physiologic mucus secretion may alter the
320 propensity for aerosol production in the 1-10 μ m range. Consequently, further studies
321 during active surgery are warranted. With regards to the testing of the clinical diagnostic
322 conditions, we must stress that our methodology was sensitive only to the generation of
323 airborne droplet nuclei. The study was not designed to detect the presence of virus
324 within these particles nor their infectious transmissibility. However, in the absence of
325 clear data on the minimum infectious dose of SARS-CoV-2, we believe our findings

326 should be interpreted in the most conservative context possible with respect to
327 infectious control recommendations.

328

329 **Conclusion**

330 Our study represents a systematic effort to quantify the degree of airborne aerosol
331 production associated with a variety of endonasal procedures. The surgical simulation
332 data confirm that the use of high speed drills and cautery produce the largest number of
333 particles. The clinical conditions revealed that endoscopic instrumentation, speech, and
334 sneezing all produced significant detectable airborne aerosols within only 30 seconds of
335 measurement. An intact surgical mask failed to fully protect against sneeze associated
336 contamination. Therefore, surgical VENT masks, as previously described by our group,
337 may not be sufficient when considering sub-10 μm particles. However, when applied to
338 an N95 respirator, the VENT modification retained the ability contain airborne aerosols.
339 These results suggest that while nasal endoscopy carries a risk profile similar to
340 established AGPs, barrier mask solutions offer the potential of effective source and
341 engineering controls.

342

343

344 **Figure Legends**

345

346 Figure 1: Surgical Simulation: A) Experimental setup (arrow denotes intake port). B)
347 Aerosol generation after 2-5 minutes (** $p < 0.001$). C) Particles separated by size (1-
348 $10\mu\text{m}$). D) Aerosols in the presence and absence of distal tip suction.

349

350 Figure 2: Clinical Simulation: A) Experimental setup (arrow denotes intake port). B)
351 Airborne aerosol generation during simulated clinical conditions. C) Airborne particle
352 generation under sneeze conditions with various source controls. (* $p < 0.05$, ** $p < 0.01$).

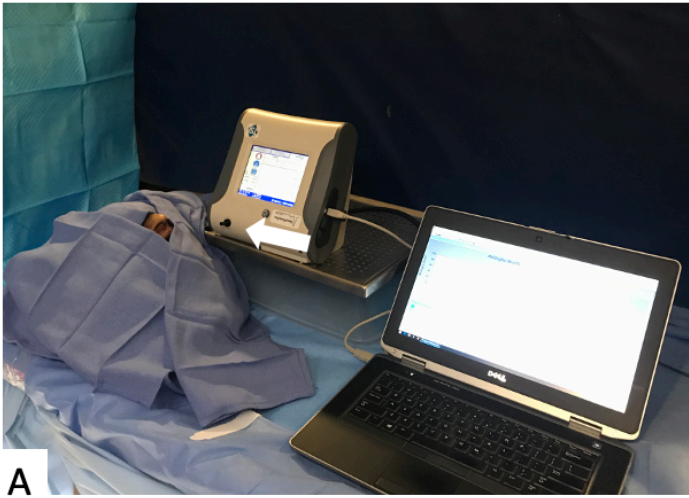
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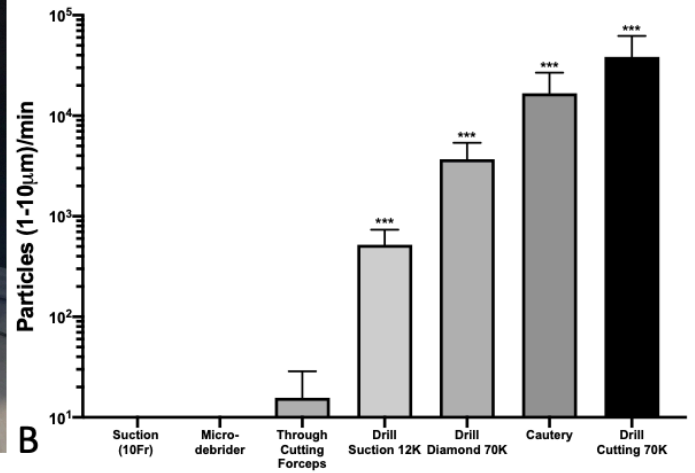
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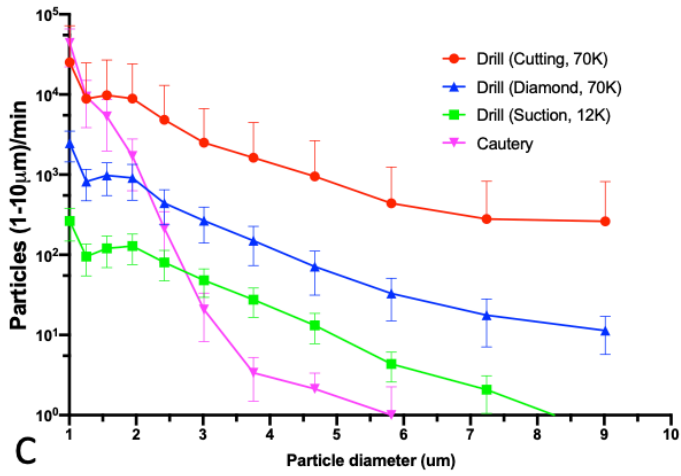
A

Airborne Aerosol Generation Under Surgical Conditions



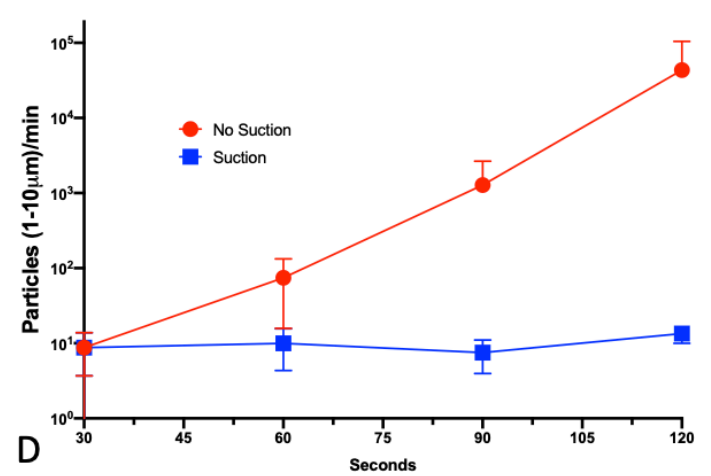
B

Airborne Aerosol Generation During Drilling Conditions



C

Airborne Aerosol Generation Under Distal Suction Conditions (12k Drill)



D

